

# Successful optical biosensing using dual optical combs: High sensitivity and rapid detection of biomolecules

September 26 2023

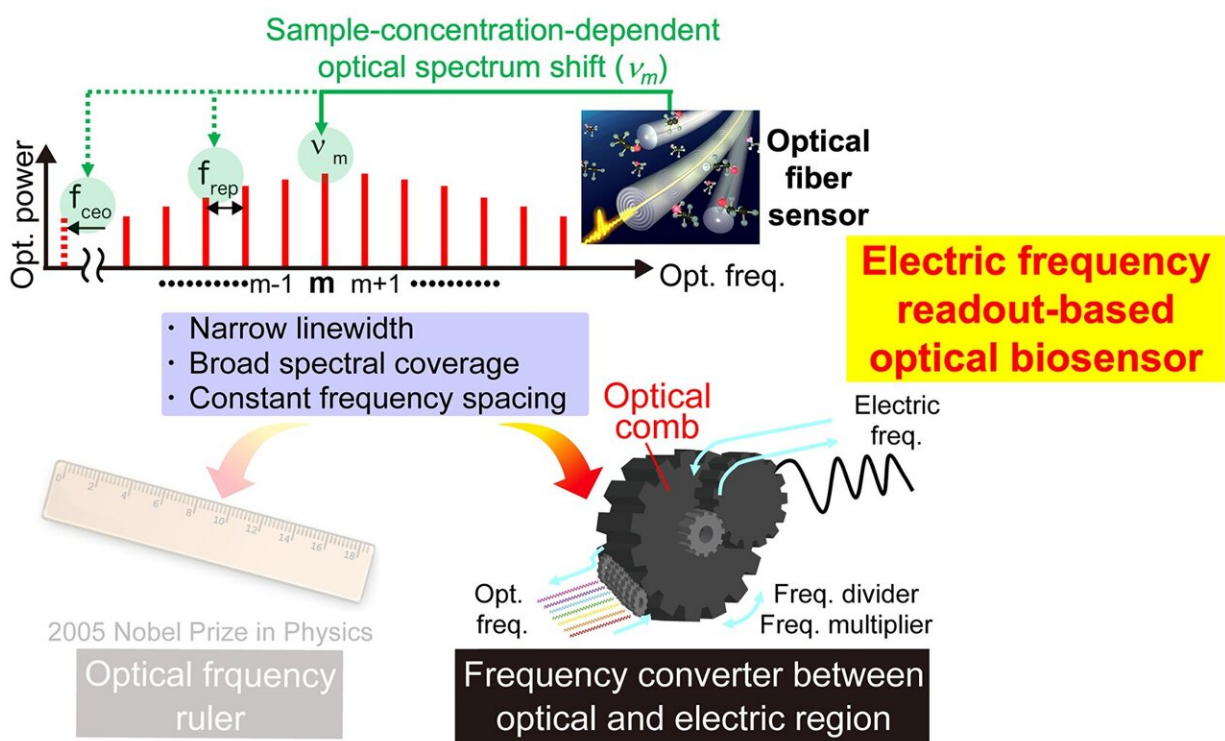


Fig 1. Electrical frequency readout-based optical biosensing using OFC. Credit: Tokushima University

Bio-sensors are biomolecular sensors that leverage or mimic the sophisticated molecular recognition capabilities of living organisms.

They find widespread applications in fields such as health care, food, and the environment.

In particular, optical biosensors, which optically read the interactions between target molecules and molecular recognition elements, offer high precision and rapid measurement capabilities. However, they have proven insufficient in terms of sensitivity for the ultra-early detection of novel coronavirus (SARS-CoV-2) and cancer cells.

A research group comprising Prof. Takeshi Yasui and visiting Associate Professor Taira Kajisa of Institute of Post-LED Photonics, Tokushima University; Doctoral Course Student Shogo Miyamura of the Graduate School of Advanced Technology and Science, Tokushima University; and Associate Prof. Shuji Taue of the School of System Engineering, Kochi University of Technology has applied [optical frequency comb](#) (OFC), which have been gaining attention as the next-generation lasers, not as light sources but as sensors for biosensing. Their work has been published in *Scientific Reports*.

In this research, the team utilized the unique optical-to-electrical [frequency](#) conversion properties of OFC in order to address the aforementioned challenges, enabling sensing in the optical frequency domain and reading out in the electrical frequency domain. Furthermore, by employing twin OFCs (dual OFC) and implementing active-dummy temperature compensation, the researchers mitigated the common issue of temperature drift in biosensing.

This breakthrough has enabled rapid and highly sensitive detection of SARS-CoV-2 and holds promise for ultras-early detection of emerging and re-emerging infectious viruses, as well as health biomarkers including cancer and environmental contaminants that pose health risks.

## **Research background and history**

Biosensors capable of detecting various biological molecules of natural origin, such as sugars, nucleic acids, and proteins, leverage or mimic the intricate molecular recognition functions of living organisms. These biomolecular sensors find applications in a wide range of fields, including health care, food, and the environment. In particular, optical biosensors that read the interactions between target molecules and molecular recognition elements optically offer features such as high sensitivity, high precision, and rapid measurements.

However, there is an ongoing need for further improvement in sensitivity. It is believed that significant enhancement of sensitivity in optical biosensors could enable ultra-early detection of novel coronavirus (SARS-CoV-2) and cancer. To achieve a substantial improvement in sensitivity, the introduction of a fundamentally different technological approach is essential.

In optical biosensing, measurements are based on the sample-concentration-dependent optical spectrum shift. However, the shift is relatively small compared to the width of the optical spectrum, and hence the performance limitations of optical spectrum measurement devices have constrained the sensitivity of biosensing.

If it were possible to convert the sample-concentration-dependent optical spectrum shift into the corresponding electrical spectrum shift for measurement, it would be feasible to achieve high sensitivity in the optical domain while providing easy handling and high-precision measurements with [electrical signals](#).

Therefore, the team turned their attention to optical frequency comb (OFC) as a means of converting optical spectrum shifts into electrical spectrum shifts.

By utilizing OFC, we can accurately convert optical frequency signals of

$10^{14}$  Hz into electrical frequency signals of  $10^8$  Hz, making it possible to perform electrical frequency signal readout-based optical biosensing using high-performance and cost-effective electrical frequency measurement equipment, they say. As a result, we are conducting research on biosensing with OFC as the core technology, which we believe holds great promise for advancing biosensing capabilities.

## Research content and results

An OFC exhibits a highly discrete multispectral structure in which numerous optical frequency modes (OFC modes) are evenly spaced like the teeth of a comb (Fig. 1, upper part). The optical frequency  $\nu_m$  of each OFC mode can be expressed by the following equation:

$$\nu_m = f_{ceo} + m f_{rep}$$

Where  $f_{ceo}$  represents the carrier-envelope-offset frequency,  $f_{rep}$  is the mode spacing, and  $m$  is the mode order. While  $\nu_m$  is an optical frequency signal of  $10^{14}$  Hz,  $f_{rep}$  and  $f_{ceo}$  are electrical frequency signals of  $10^8$  Hz. This equation signifies the connection between optical and electrical frequency signals through the OFC.

For example, by phase-locking  $f_{rep}$  and  $f_{ceo}$  to an electrical frequency standard through laser control, the uncertainty of the electrical frequency standard can be transferred to  $\nu_m$ , allowing the OFC to serve as "optical frequency ruler" secured by the electric frequency standard (Fig. 1, bottom left).

Conversely, this relationship can be utilized to convert optical frequency signals into electrical frequency signals. For instance, placing a fiber biosensor within the resonator of a fiber OFC enables the conversion of sample-concentration-dependent optical frequency spectrum shifts ( $\nu_m$  shift) into electrical frequency spectrum shifts ( $f_{rep}$  shift) (Fig. 1, bottom

right).

Electrical frequency signal benefits from the availability of highly accurate national standards and the existence of high-performance, cost-effective measurement equipment, enabling high-precision, wide-dynamic-range, fast, and convenient measurements.

By leveraging the excellent synergy between "optical-to-electrical frequency conversion in OFC " and "high-precision electrical frequency measurement," we have successfully enabled electrical frequency readout-based optical biosensing (biosensing OFC). This novel approach combines the high sensitivity of the optical frequency domain with the ease of handling and precision of electrical frequency readouts.

One of the remaining challenges in biosensing OFC is the temperature drift in the sensor signal of  $f_{rep}$ .  $f_{rep}$  is determined by the reciprocal of the optical resonator length of the fiber OFC, and it varies due to changes in environmental temperature, which cause thermal expansion and contraction of the optical resonator length.

This temperature-induced variation in  $f_{rep}$  is superimposed on the sensor signal as temperature drift. Since the  $f_{rep}$  variation caused by temperature drift is often larger than the  $f_{rep}$  shift due to changes in sample concentration, an active-dummy temperature compensation approach has been employed (Fig. 2).

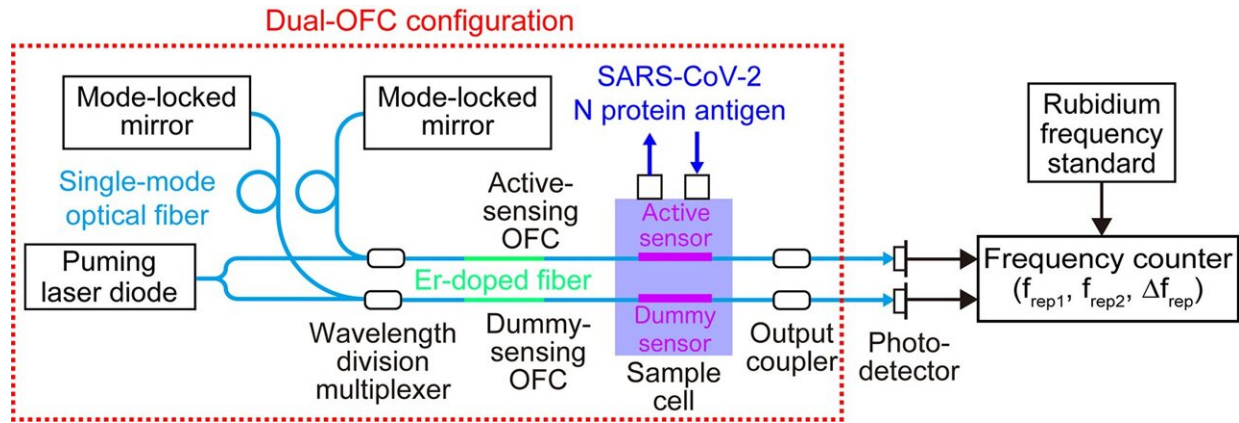


Fig 2. Active-dummy temperature compensation utilizing dual OFC. Credit: Tokushima University

In this method, equivalent fiber OFC resonators are prepared in pairs (dual OFC). One of the cavities (active-sensing OFC, mode spacing =  $f_{rep1}$ ) incorporates a fiber sensor with surface modifications for biosensing (active sensor), while the other cavity (dummy-sensing OFC, mode spacing =  $f_{rep2}$ ) remains another fiber sensor without surface modifications (dummy sensor). As both sensors are placed in the same sample cell, only the active sensor is sensitive to the antigen, while the effect of temperature drift is observed similarly in both sensors.

Therefore, by measuring the differential signal between the active-sensing OFC and the dummy-sensing OFC ( $\Delta f_{rep} = f_{rep1} - f_{rep2}$ ), it becomes possible to compensate for the influence of temperature drift and extract only the signal dependent on sample concentration. This innovative approach significantly improves the accuracy and reliability of the biosensing OFC, allowing for precise and real-time detection of biological molecules while mitigating the effects of temperature fluctuations.



In this experiment, we conducted measurements while incrementally varying the concentration of the SARS-CoV-2 nucleocapsid (N) protein antigen in phosphate-buffered saline (PBS) at 10-minute intervals.

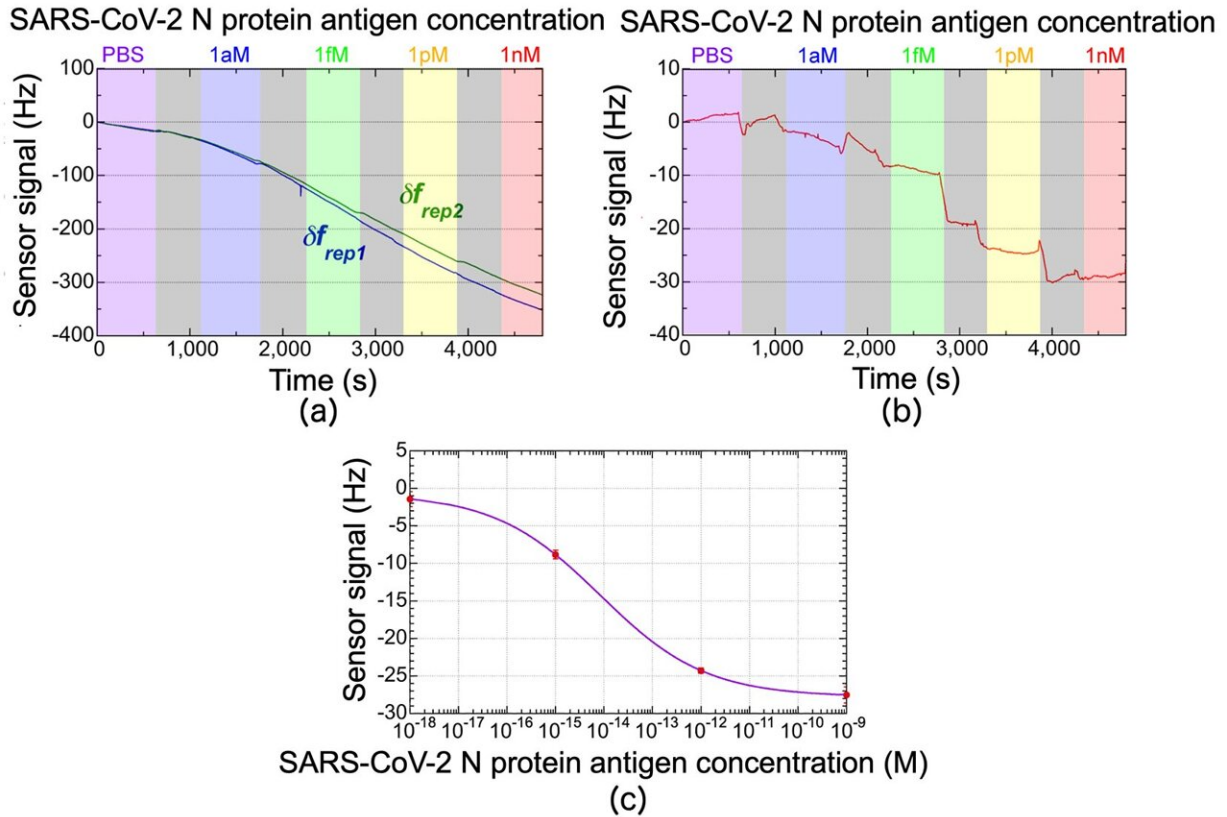


Fig 3. Experimental results. Credit: Tokushima University

Figure 3(a) illustrates the changes in sensor signals ( $f_{rep1}$  and  $f_{rep2}$ ) from the active-sensing OFC and the dummy-sensing OFC. In both sensor signals, a gradual change due to temperature drift is observed, but there is no evidence of step-wise changes related to antigen concentration in the active-sensing OFC signal. This is attributed to the fact that the temperature-induced variations in  $f_{rep}$  are more significant than the  $f_{rep}$

shifts caused by changes in antigen concentration.

Then, the extracted differential signal ( $\Delta f_{rep}$ ) between the two sensors is presented in Fig. 3(b). The temperature drift is effectively suppressed, and the step-wise changes corresponding to antigen concentration are clearly evident. From the measurement results, we generated a graph illustrating the relationship between antigen molar concentration and sensor signal, as shown by the red circle plots in Fig. 3(c).

To assess the validity of the experimental results, we performed curve fitting analysis using a theoretical model (purple line). The analysis confirmed that within a 10-minute measurement time, the detection limit for molar concentration is 37aM. This rigorous validation underscores the accuracy and reliability of our biosensing approach and its remarkable sensitivity in detecting extremely low concentrations of the SARS-CoV-2 N protein antigen.

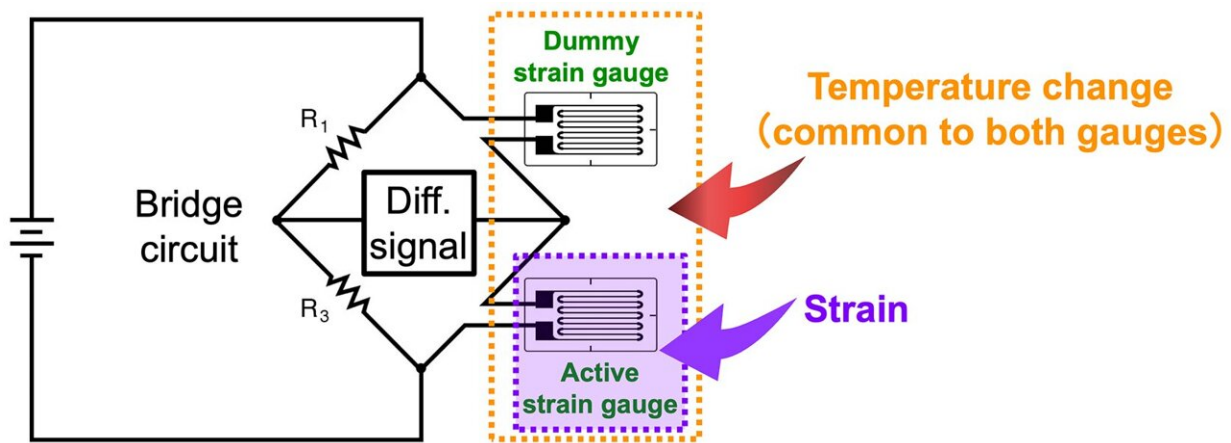


Fig A. Credit: Tokushima University



## Future developments

While this measurement was conducted under ideal conditions with only the SARS-CoV-2 protein antigen present in PBS, real-world samples (such as saliva, nasopharyngeal swabs, and nasal swabs) often contain a multitude of unwanted proteins (interfering substances) due to non-specific adsorption. This non-specific adsorption can limit sensitivity and precision.

In our future work, we plan to consider actual samples and implement sensor surface modification methods that prevent non-specific adsorption. This will allow us to assess the performance under conditions that closely resemble real-world scenarios and ensure the accuracy and reliability of our biosensing technology for practical applications.

**More information:** Shogo Miyamura et al, Rapid, high-sensitivity detection of biomolecules using dual-comb biosensing, *Scientific Reports* (2023). [DOI: 10.1038/s41598-023-41436-3](https://doi.org/10.1038/s41598-023-41436-3)

Provided by Tokushima University

Citation: Successful optical biosensing using dual optical combs: High sensitivity and rapid detection of biomolecules (2023, September 26) retrieved 10 May 2024 from <https://phys.org/news/2023-09-successful-optical-biosensing-dual-high.html>

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