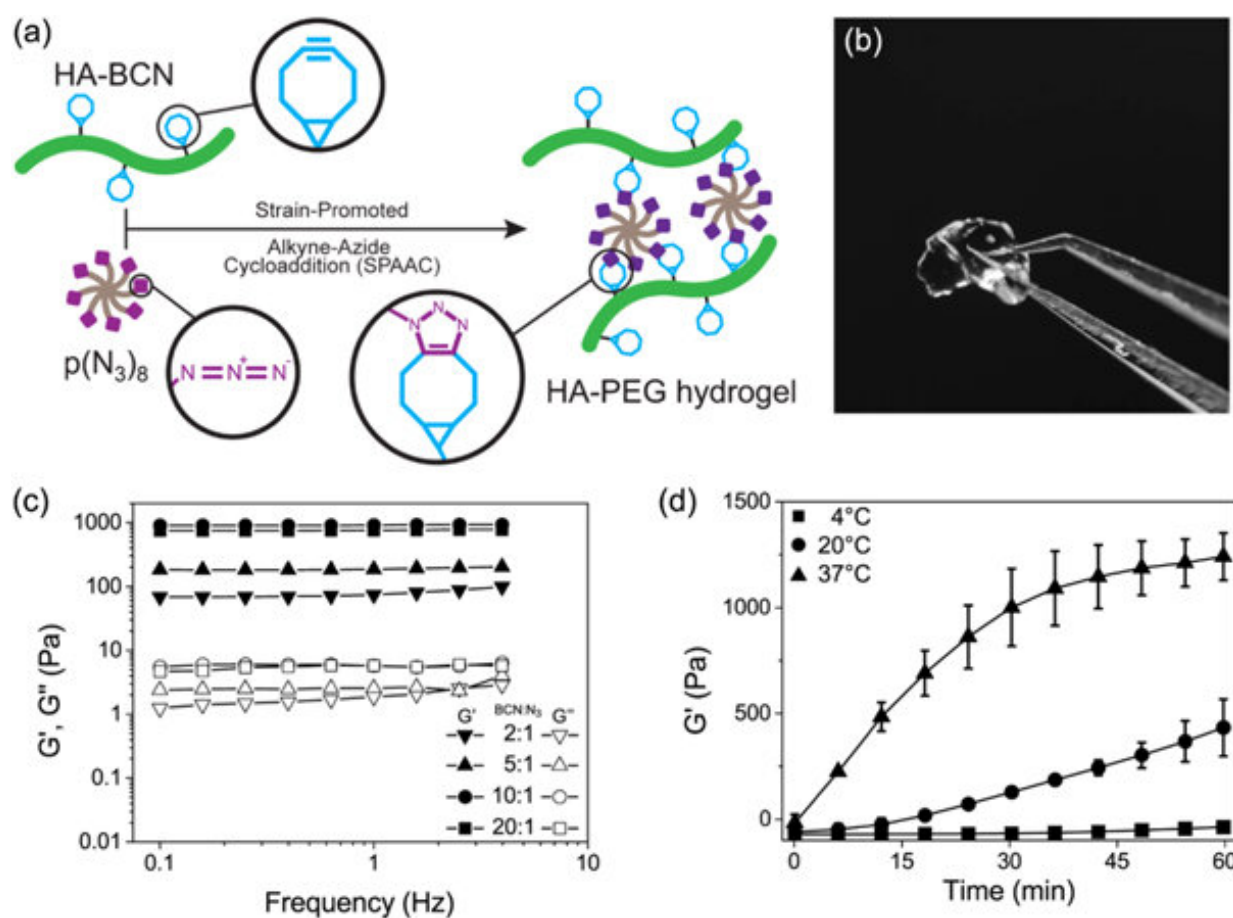


# 3-D culturing hepatocytes on a liver-on-a-chip device

January 17 2019, by Thamarasee Jeewandara



(a) Schematic representation of the formation of HA-PEG hydrogels through a strain-promoted alkyne-azide cycloaddition reaction. (b) Photograph of a HA-PEG hydrogel after formation. (c) Frequency sweeps of HA-PEG hydrogels with different BCN to N<sub>3</sub> ratios. (d) Gelation time experiment showing the increase of  $G'$  over time during gelation of HA-PEG hydrogels (10:1 BCN:N<sub>3</sub>) at different temperatures. Credit: *Biofabrication*, doi:

<https://doi.org/10.1088/1758-5090/aaf657>

Liver-on-a-chip cell culture devices are attractive biomimetic models in [drug discovery](#), [toxicology](#) and [tissue engineering](#) research. To maintain specific liver cell functions on a chip in the lab, adequate cell types and culture conditions must be met, which includes 3D cell orientation and a consistent supply of nutrients and oxygen. Compared with conventional 2D cell culture techniques, [organ-on-a-chip devices](#) offer versatility and effective biomimicry suited for advanced applications in drug discovery and medicine.

In a recent study now published on *Biofabrication*, Jonas Christoffersson and colleagues demonstrated how hydrogels that mimic the [extracellular matrix](#) can support the functionality and viability of [hepatocytes](#) in a perfused liver-on-a-chip device. The interdisciplinary researchers in the division of biotechnology and molecular physics engineered a [hydrogel](#) system based on hyaluronan and poly(ethylene glycol) (HA-PEG) polymers. They developed the hydrogels using [click chemistry](#). To enable the process, the [scientists](#) conducted a biorthogonal reaction (chemistry that occurs within living systems without the interference of native biochemical reactions) between a [cyclooctyne](#) moiety and alkyne azide-labelled reaction partner, known as strain-promoted alkyne azide cycloaddition (SPAAC).

The new hydrogel materials were engineered and characterized in comparison with existing agarose and alginate hydrogels for cell compatibility (cytocompatibility). For biofunctionalization studies, the researchers used human [induced-pluripotent](#) stem cell derived [hepatocytes](#) (hiPS-HEPs). To improve surface cytocompatibility of the biomaterial, HA-PEG hydrogels were altered with azide-modified cell adhesion motifs to facilitate effective cell-material attachments. In the

surface functionalized biomaterial, the hepatocyte stem cells migrated and grew in 3D orientations, with increased viability. The scientists observed higher albumin production on the novel material (characteristic liver protein), compared to cells cultured on other hydrogels. The flexible, SPAAC crosslinked hydrogel system with perfused 3D cell culture of hiPS-HEPs is a promising material to optimize liver-on-a-chip devices.

Miniaturized bioreactors known as '[organ-on-chips](#)', have recently emerged as alternative cell culture models that better mimic the in vivo biological microenvironment in the lab. The liver is a model of special interest in medical research due to [drug hepatotoxicity](#) observed at all phases of [clinical drug development](#). Previous publications detail the use of organ-on-chips to predict the outcome of a drug's impact in clinical trials and evaluate [drug interactions with hepatocytes](#) in the lab.

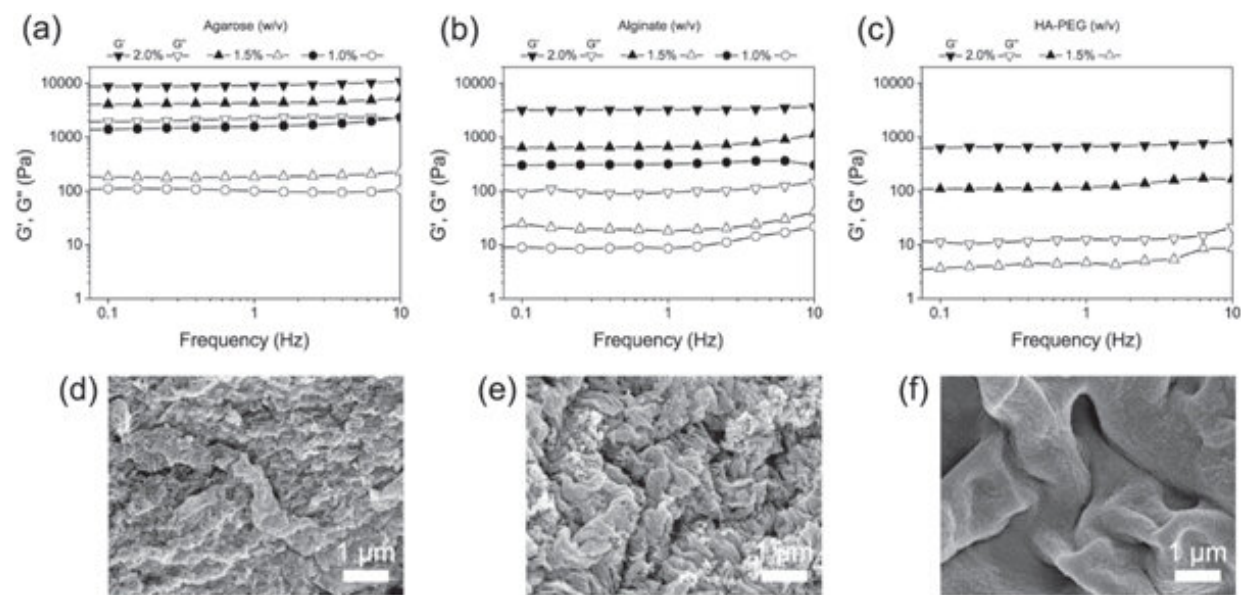


Structure of a) HA-BCN with a ratio n/m of 0.19 and b) p(N<sub>3</sub>)<sub>8</sub>. Credit: *Biofabrication*, doi: <https://doi.org/10.1088/1758-5090/aaf657>

Due to their wider adoption in academic and industrial settings, the bioreactors require optimized materials and conditions for high throughput fabrication. Conditions include replacing the common prototyping material polydimethylsiloxane (PDMS), integrating induced [pluripotent stem cell](#) (iPSC)-derived cells on a soft biomaterial that facilitates their growth and minimizing the large dead volume caused by [microfluidics](#) reservoirs and tubing of organ-on-chips devices.

The novel biomaterial prepared in the study contained two main constituents crosslinked via SPAAC; a cyclooctyne-modified hyaluronan (HA-BCN) and a multiarmed azide-modified PEG [p(N<sub>3</sub>)<sub>8</sub>]. The BCN reacted with azides (N<sub>3</sub>) on the 8-armed PEG polymer with terminating N<sub>3</sub>-moieties to form a stable 1,2,3-triazole. Christoffersson et al. completed chemical reactions under physiological conditions to form the hydrogels with tunable viscoelastic properties. The crosslinking strategy was ideal to fabricate hydrogels for 3D cell culture; as the cells could be encapsulated in the biomaterial without compromising their viability and were suitable for use in microfluidic devices. The scientists used excess SPAAC moieties on the novel biomaterial to attach different ligands including [RGD peptides](#) to promote interactions at the cell-material interface.

Thereafter, the scientists varied the composition of the two main constituents to understand the resulting viscoelastic properties, such as [the storage modulus](#) (G') and loss modulus (G'') of the hydrogels via oscillatory rheology (technique to measure the viscoelastic behavior of soft materials). They controlled the gelation kinetics of the novel hydrogel at increasing temperatures. [Gelation kinetics](#) of the new [biomaterial](#) was slow enough for homogenous cell distribution but rapid enough to prevent cell sedimentation. The ability to control gelation kinetics allowed the scientists to consider a variety of biofabrication strategies (e.g. bioprinting) and hydrogel assembly within the microfluidic systems for organ-on-chip applications.



(a)–(c) Frequency sweeps of (a) agarose, (b) alginate and (c) HA-PEG hydrogels at different concentrations. (d)–(f) SEM micrographs of (d) agarose, (e) alginate and (f) HA-PEG hydrogels showing the morphology of each hydrogel. Credit: *Biofabrication*, doi: <https://doi.org/10.1088/1758-5090/aaf657>

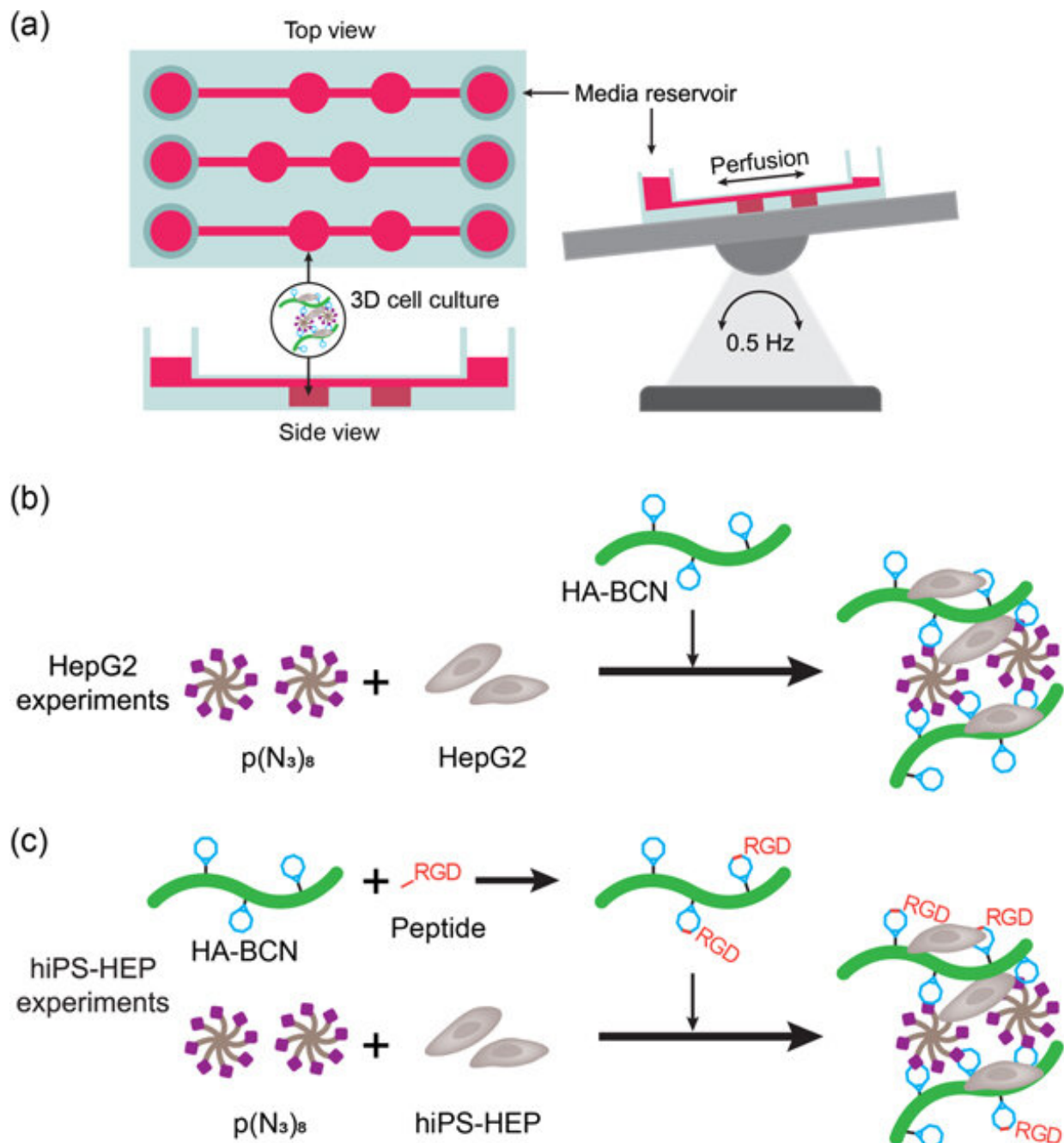
Christoffersson et al. next compared the HA-PEG hydrogels with the well-established 3D cell culture scaffolds - agarose and alginate hydrogels. In order to determine the final viscoelastic properties suited for 3D cell culture experiments, they used oscillatory rheology to examine the different polymer concentrations. The scientists analyzed the composition of the finalized materials using scanning electron microscopy (SEM) images.

The liver-on-a-chip design and setup had to meet two key criteria in the study:

1. Allow perfusion (passage of fluid) of cell culture medium across the

hydrogel surface for steady nutrient media exchange, to and from the encapsulated hepatocytes.

2. Allow sampling of the perfused media for experimental analysis during ongoing cell culture, without affecting the hepatocytes and the hydrogel.





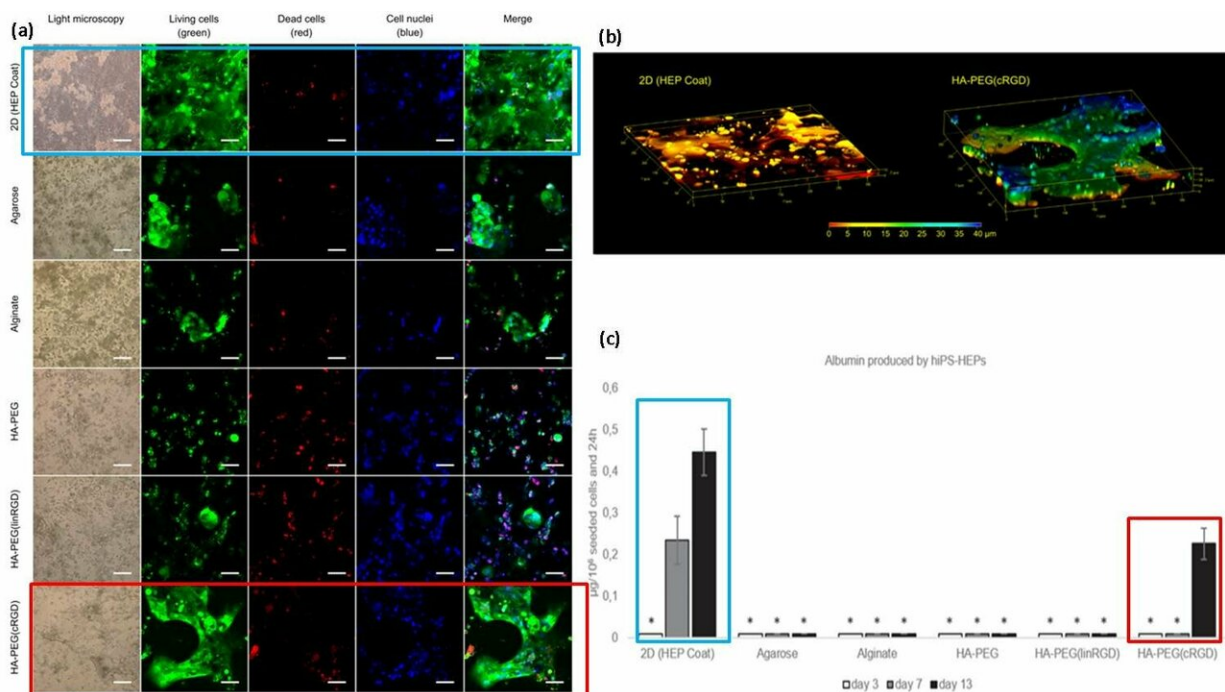
(a) Schematic representation of the liver-on-a-chip device and setup. The device was put on an automatic rocker table to allow perfusion of media and nutrients during cell culture. (b) Depiction of the HepG2 3D cell culture experiments with HA-PEG hydrogels. The HepG2 cells were added to media-suspended p(N3)8 prior addition of HA-BCN. (c) Depiction of the hiPS-HEP 3D cell culture experiments with HA-PEG hydrogels. The hiPS-HEP cells were added to media-suspended p(N3)8 prior addition of HA-BCN. In experiments using either linRGD or cRGD peptide, the HA-BCN was preincubated with 1  $\mu$ M of corresponding peptide for 1 h prior adding the HA-BCN(RGD) component to the hiPS-HEP/p(N3)8 mixture. Credit: *Biofabrication*, doi: <https://doi.org/10.1088/1758-5090/aaf657>

To meet these criteria, the scientists used a commercial [3D cell culture device](#) ( $\mu$ -Slide III 3D Perfusion IbiTreat) containing two consecutive chambers (2 x 30  $\mu$ L) in three parallel arrays - each connected to media reservoirs to perfuse liquid. For effective perfusion, they mounted the device on an automatic rocking table by reversing the perfusate direction across the hydrogel-containing chambers. The experimental setup allowed perfusion through the device, fulfilling the first criteria. To fulfill the second criteria, the localized walls adjacent to the hydrogel chambers allowed the scientists to sample the perfusate without interfering the hydrogel or cell constituents.

The scientists first investigated biofunctionalization of liver-on-a-chip devices in the study with HEPG2 cells (liver carcinoma cell line) encapsulated in hydrogels, after 3, 7 and 9 days of cell culture. They compared the cell morphology, viability and functionality with agarose and alginate hydrogels. The study included live/dead assays to confirm cell viability and further confirmed HepG2 functionality by detecting albumin and urea secretions in the supernatant of the cell culture.

For improved cell functionality (surface attachment and mobility on materials), the scientists grafted cell adhesion motifs such as linear or cyclic [RGD peptides](#) (linear linRGD or cyclic cRGD) on to the hydrogels. In this instance, hiPS-HEP cells (hepatocyte stem cells) were cultured across different hydrogel compositions for 13 days to examine the morphology and viability (live/dead staining) after cell-material interactions. The scientists used six different hydrogel-based biomaterial surfaces in the experiments including; 2D (HEP coat), Agarose, Alginate, HA-PEG, HA-PEG (linRGD) and HA-PEG (cRGD).

The hiPS-HEP cells encapsulated and cultured in the modified hydrogel grew within 2D and true 3D constructs. To test the functionality of the cultured hiPS-HEP cells (stem cells), the scientists quantified their albumin and urea excretion. The results showed that only the supernatants of stem [cells](#) cultured in 2D surfaces and in the presence of the cRGD motif hydrogels secreted albumin.





(a) Viability and morphology of hiPS-HEP cells after 13 days of culture. Cell viability seems to be dependent on the cell's ability to attach to the surface, the hydrogel, or to each other. Large structures of hiPS-HEPs were formed in HA-PEG(cRGD). (calcein, green), dead cells (ethidium homodimer-1, red), and nuclei (Hoechst 33 342, blue). (b) Z-stack of images obtained by confocal microscopy reveals the flat shape of hiPS-HEPS when cultured on a 2D substrate (left) compared to the 3D constructs of the cells in a HA-PEG(cRGD) hydrogel (right). The colours represent the height above the 3D cell culture device chamber bottom, i.e. the Z-axis, from 0  $\mu\text{m}$  (red) to 40  $\mu\text{m}$  (blue). (c) Albumin produced by hiPS-HEP on HEP Coat in 2D and in the different hydrogels. \* indicates that the albumin concentration levels were too low for reliable quantification. Credit: *Biofabrication*, doi: <https://doi.org/10.1088/1758-5090/aaf657>

Based on the results, the scientists attributed the higher albumin quantity on the 2D HEP coat to the rate of albumin diffusion within hydrogels; transfer across 2D coat being faster than 3D. The higher concentration of albumin with cRGD motif bound hydrogels, correlated with the increased cell growth and viability observed on the cRGD bound biomaterial surfaces. As a result, the scientists intend to use cyclic forms of RGD peptide to assist hepatocyte stem cell culture on hydrogels prepared for liver-on-a-chip devices in the future.

In this way, the study detailed the advantages of using hyaluronan-PEG based hydrogel modified with RGD peptides for 3D cultures of hepatocytes (approximating 13 days) in a liver-on-a-chip setup. As benchmarks of the study, Christofferfsson and co-workers used the commonly available alginate and agarose hydrogels. In the future, the scientists will optimize the viscoelastic properties and the concentration of cell adhesion motifs on the HA-PEG hydrogel system for biomimetic cytocompatibility. The optimized [hydrogel](#) system can be combined with the device setup to facilitate physiologically relevant liver-on-a-chip

platforms for clinical research in drug toxicology, drug discovery and regenerative medicine.

**More information:** 1. Fabrication of modular hyaluronan-PEG hydrogels to support 3D cultures of hepatocytes in a perfused liver-on-a-chip device [iopscience.iop.org/article/10.1088/1758-5090/aaf657](https://iopscience.iop.org/article/10.1088/1758-5090/aaf657), Jonas Christoffersson et al. 27 December 2018, *Biofabrication*, *IOP Science*.

2. Controlling hydrogelation kinetics by peptide design for three-dimensional encapsulation and injectable delivery of cells [www.pnas.org/content/104/19/7791](https://www.pnas.org/content/104/19/7791) Haines-Butterick L. et al. May 2007, *PNAS*.

3. Microfluidic organs-on-chips [www.nature.com/articles/nbt.2989](https://www.nature.com/articles/nbt.2989) Bhattia S. N and Ingber D.E. August 2014, *Nature Biotechnology*.

4. Organs-on-chips at the frontiers of drug discovery, [www.nature.com/articles/nrd4539](https://www.nature.com/articles/nrd4539) Esch E.W. et al. March 2015, *Nature Reviews Drug Discovery*.

© 2019 Science X Network

Citation: 3-D culturing hepatocytes on a liver-on-a-chip device (2019, January 17) retrieved 10 April 2024 from <https://phys.org/news/2019-01-d-culturing-hepatocytes-liver-on-a-chip-device.html>

This document is subject to copyright. Apart from any fair dealing for the purpose of private study or research, no part may be reproduced without the written permission. The content is provided for information purposes only.